



# Optimisation of CT radiation dose in PET/CT imaging using mA modulation and iterative reconstruction

**CTUG Meeting**

**16<sup>th</sup> October 2014**

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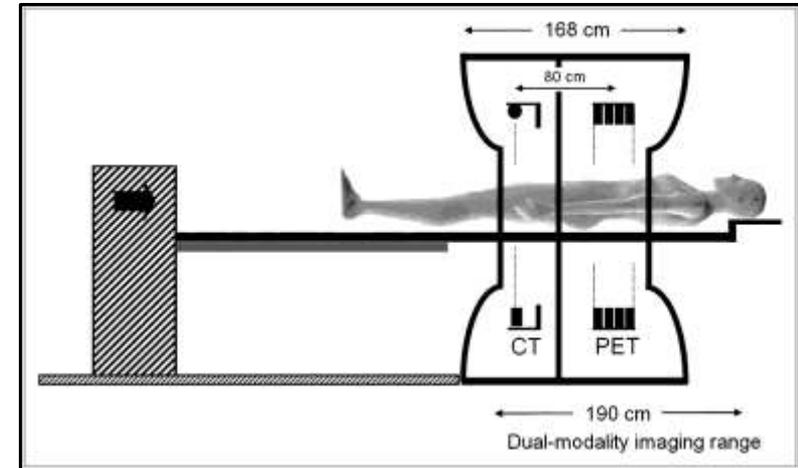
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# Introduction

## CT in PET-CT

- Patients administered with tracer compound labelled with positron emitting radionuclide i.e.  $^{18}\text{F}$ -FDG
- Uptake period of 90 minutes in holding bay
- Patient has half-body CT scan (<1 minute) followed by half-body PET imaging (3 min/bed position ~ 21 minutes)



Dispensing PET tracer



Patient Administration and Uptake



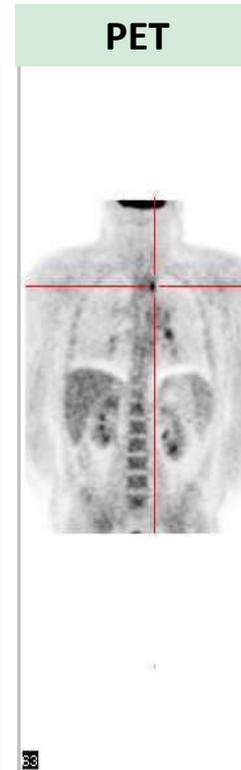
PET-CT Scanning



# Introduction

## CT in PET-CT

CT Protocol	
mA	115
Rotation Speed	0.5s
Pitch	1.375
Collimation	16 x 2.5mm
CTDI <sub>vol</sub>	5.2mGy



PET Protocol	
ARSAC Diagnostic Reference Level (DRL) <sup>18</sup> F-FDG	400MBq
Effective Dose 400MBq <sup>18</sup> F-FDG	8mSv

CT Radiation dose = 7mSv

PET Radiation dose for 350MBq <sup>18</sup>F-FDG = 7mSv

# Introduction

## Aims



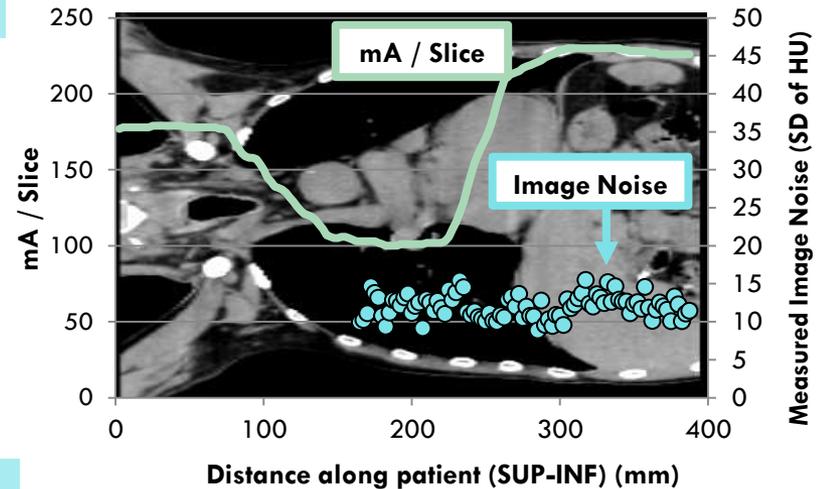
- PET Imaging Centre at St. Thomas' Hospital moved to new area in hospital in Oct 2013
- 2 x GE Discovery 710 PET-CT scanners (Optima 660 CT component)
- New scanners have mA modulation and statistical iterative reconstruction
- For optimisation of PET and CT protocols, institutional ethical approval obtained to perform patient local views on new scanners with patients receiving no additional radiation dose;



# Introduction

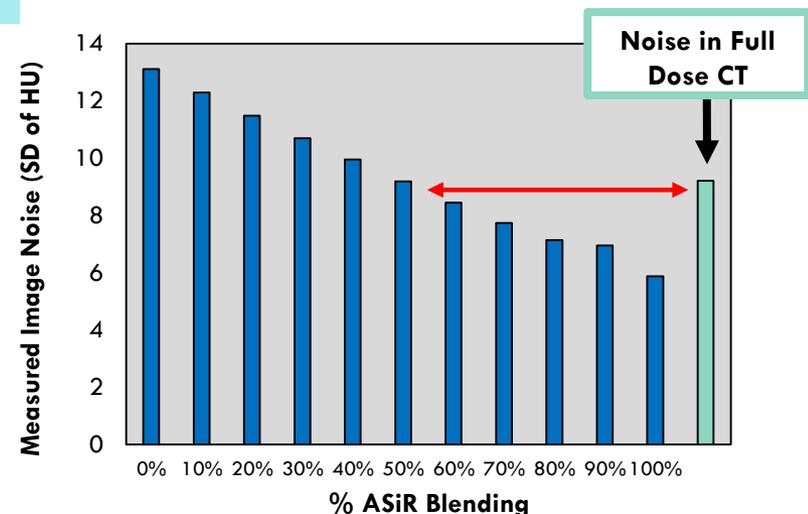
## GE Smart mA

- CT tube current varies rotationally and longitudinally as patient is scanned to maintain image noise constant
- Parameters to set are minimum mA, maximum mA and Noise Index



## GE ASiR (Adaptive Statistical Iterative Reconstruction)

- System noise statistics model applied to original projection data; Noise propagated through to iteratively reduce noise in reconstructed images.
- Statistical reconstruction is blended to various degrees with the original FBP reconstruction. GE recommend a setting of 40% ASiR blending, which theoretically enables a 40% dose reduction with no change in image noise.



Variation of measured image noise in water with % ASiR for a 50% reduced dose CT

# Methodology

## **A: Local view CT scans to determine optimum Noise Index (NI)**

Patient local views (N=13) were scanned with the NI set to obtain a  $CTDI_{vol}$  value 50% that of the current protocol. All images were reconstructed using 40% ASiR.

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## B. Clinician review of Low Dose Scans

CT local views stored alongside several full dose FBP only CT images of patients of matched size and appearance. Images were scored blindly for image quality by 3 PET/CT clinicians, using scoring scale:

- 1 = non-diagnostic or unacceptable
- 2 = diagnostic but sub-optimal
- 3 = satisfactory
- 4 = good
- 5 = excellent

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## **C: Proposed protocol**

The results from Part A and Part B were used to define a reduced dose CT protocol, and an additional 7 patients were scanned.

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## D: Evaluation of Final Images

The local views obtained in Part C were reviewed again by clinicians to assess the proposed protocol. Any variations/changes to the proposed protocol were discussed.

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## E: Clinical Implementation of New Protocol

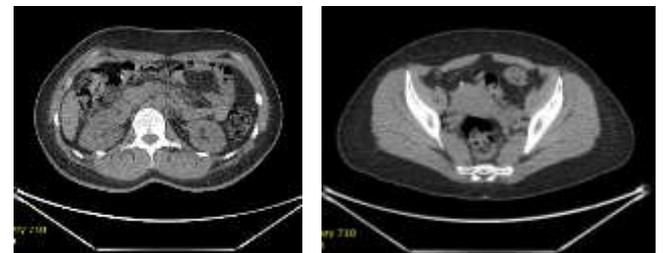
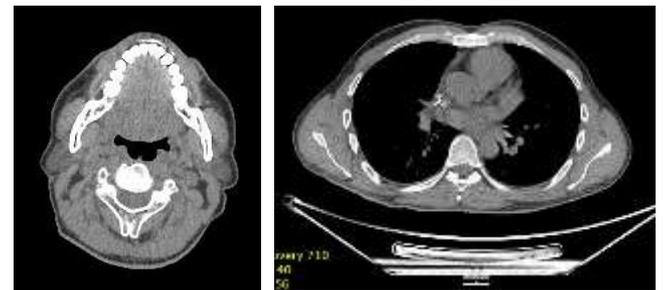
Scanning protocols changed on scanner. New temporary DRLs were set and staff received training in mA modulation/patient centering prior to first patient scans using new protocol.

# Results

## Clinician Scoring of Part A Images

	Clinician A	Clinician B	Clinician C
Head and Neck 1	4	3	3
Head and Neck 2	4	3	4
Chest 1	4	4	5
Chest 2	5	4	3
Chest 3	3	3	2
Chest 4	3	2	3
Abdo 1	5	4	4
Abdo 2	4	3	3
Pelvis 1	4	3	2
Pelvis 2	5	3	3
Pelvis 3	4	2	3
Pelvis 4	4	3	4

Scoring Scale	
1	Non-diagnostic or unacceptable
2	Diagnostic but sub-optimal
3	Satisfactory
4	Good
5	Excellent



# Results

## Clinician Scoring of Part A Images

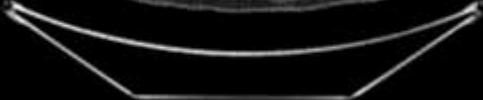
	Clinician A	Clinician B	Clinician C
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Chest 1	4	4	5
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- None of the Part A local view images scanned at 50% dose were deemed **'non-diagnostic or unacceptable'**
- **Weighted Kappa Test:**
  - Fair correlation between Clinician A and Clinician B,
  - Fair correlation between Clinician B and Clinician C
  - No correlation between Clinician A and Clinician C.

# Results

## Clinician Scoring of Part A Images

	Clinician B	Clinician C
	3	3
	3	4
	4	5
	4	3
	3	2
	2	3
	4	4
	3	3
	3	2
	3	3
	2	3
	3	4

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- **Diagnostic but sub-optimal:** patients scanned with arms down, pacemaker artefacts, large patients

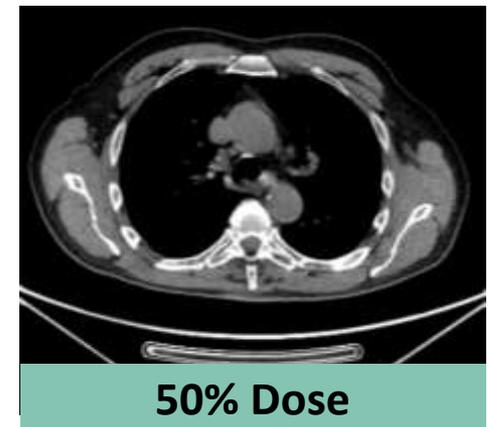
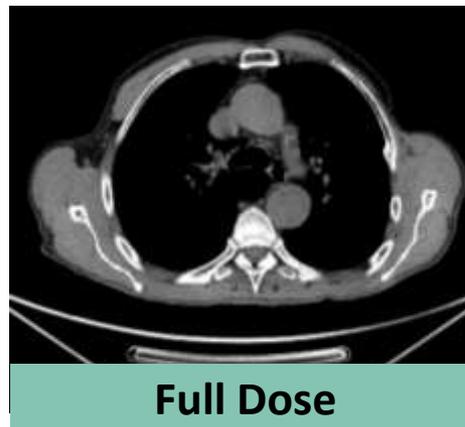
# Results

## Clinician Scoring of Part A Images

- 'Matched' CT images

	Clinician A Scores		Clinician B Scores		Clinician C Scores	
	Full Dose	50% Dose	Full Dose	50% Dose	Full Dose	50% Dose
Chest	4	4	5	4	5	5
Abdo	4	4	4	3	3	3
Pelvis	4	4	4	4	4	4
Head and Neck a)	4	4	4	3	4	3
Head and Neck b)	4	4	4	3	5	4

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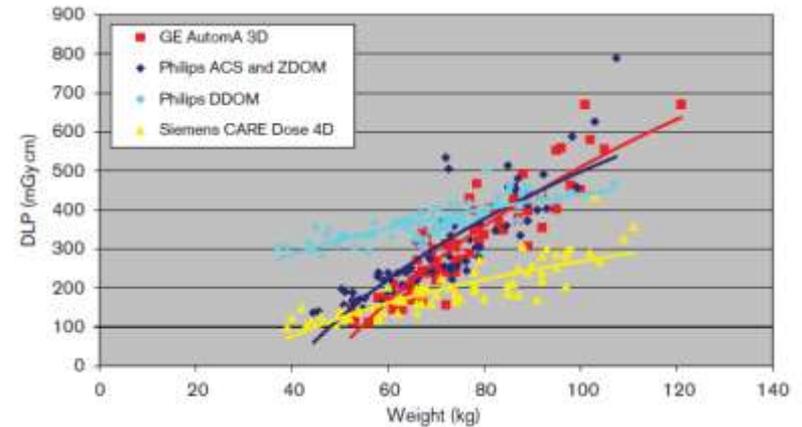


# Results

## Proposed Protocol: Torso

- Mean GE Noise Index (NI) 50% dose reduction was **41** (1 S.D. = 6, Range 34 – 52)
- Proposed protocol:

<b>Noise Index</b>	40
<b>Minimum mA</b>	15
<b>Maximum mA</b>	100
<b>Acquired Slice Thickness</b>	2.5mm
<b>Reconstruction</b>	Std/40% ASiR



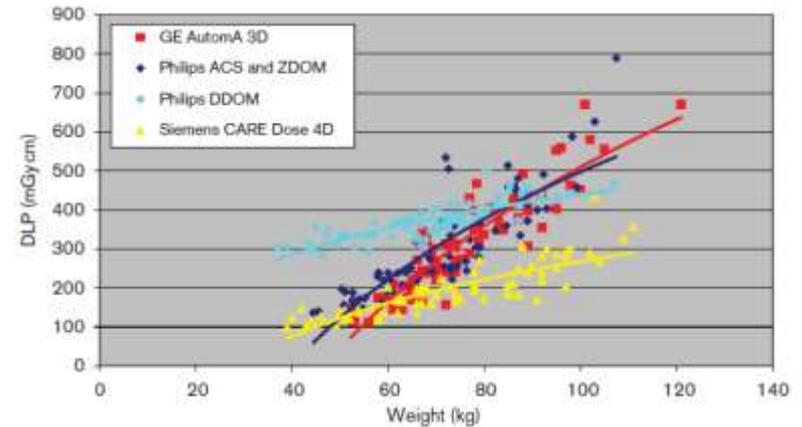
G Iball and D Tout, *Computed Tomography Automated Exposure Control Techniques in <sup>18</sup>F-FDG Oncology PET-CT Scanning*, Nuc Med Comm 2014, Vol 35 No 4

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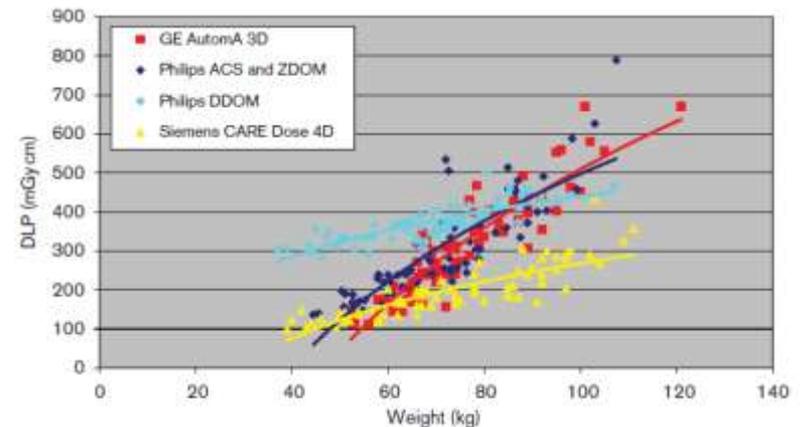
- Protocol was tested on scanners without scanning for a selection of 11 patients. The mean displayed  $CTDI_{vol}$  (2.9mGy) represented a 45% dose reduction compared to the current fixed mAs protocol; mA saturated at 100mA for 8/11 patients;

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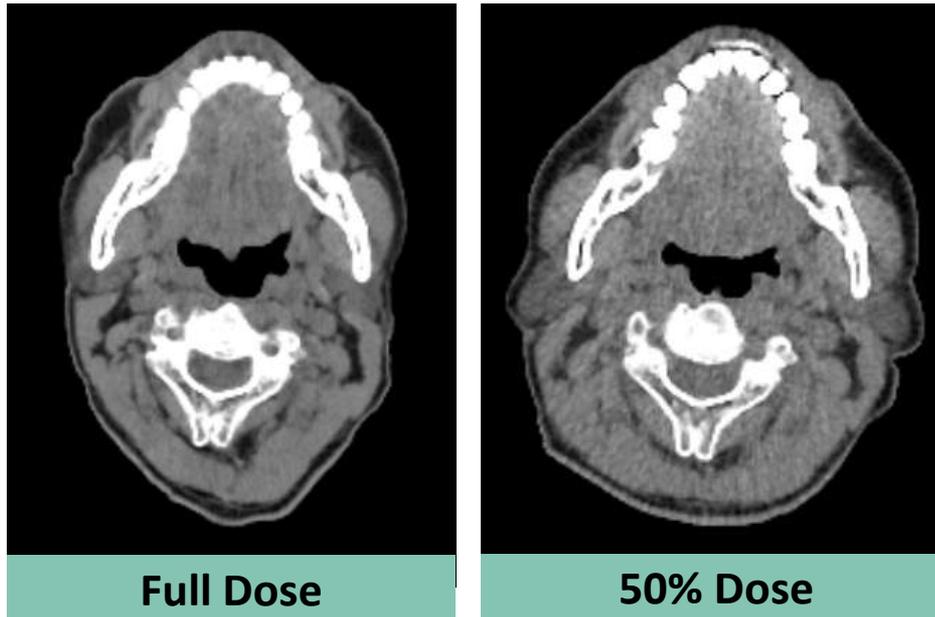


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- For remaining 4 torso local view patients, small patients (<50kg) were scanned.
- In evaluation of the final images, clinicians were satisfied with the image quality and therefore one protocol used for all patient sizes.

# Results

## Proposed Protocol: Head and Neck

- Head and neck region represents a challenge to mA modulation.

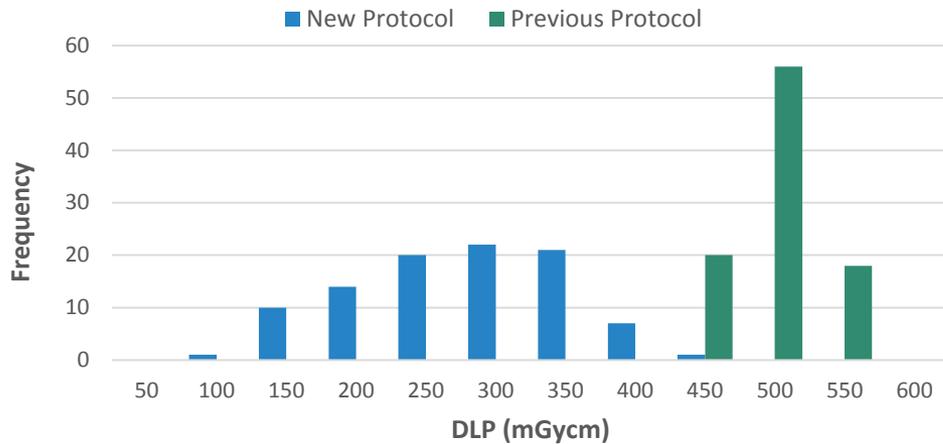


- As 2/3 clinicians scored the reduced dose head and neck image quality down in the initial images, in second group of scans the Noise Index and minimum mA were varied to improve image quality.
- In clinician review of the final images, it was concluded that the mA modulation ASiR protocol would not be implemented for these scans.

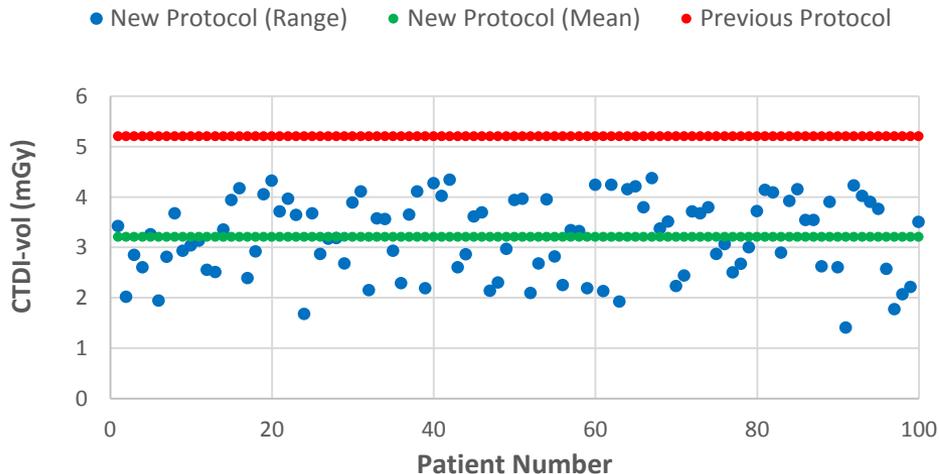
# Results

## Dose Reduction of New Protocol

DLP: Comparison of Protocols



CTDI<sub>vol</sub>: Comparison of Protocols



	Old Protocol	New Protocol
	DLP (mGycm)	DLP(mGycm)
<b>Mean</b>	486	302
<b>Std Dev</b>	64	77
<b>Max</b>	852	467
<b>Min</b>	416	114
<b>Third Quartile</b>	479	363
<b>Mean Dose Reduction (range)</b>		38% (4% - 77%)

	Old Protocol	New Protocol
	CTDI <sub>vol</sub> (mGy)	CTDI <sub>vol</sub> (mGy)
<b>Mean</b>	5.2	3.2
<b>Std Dev</b>	----	0.8
<b>Max</b>	----	4.4
<b>Min</b>	----	1.4
<b>Third Quartile</b>	----	3.9
<b>Mean Dose Reduction (range)</b>		38% (15% - 73%)

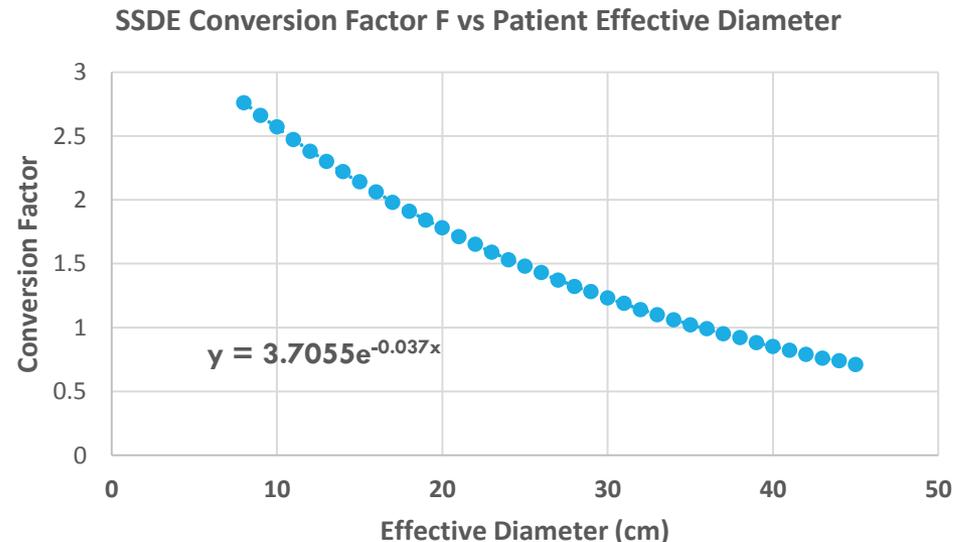
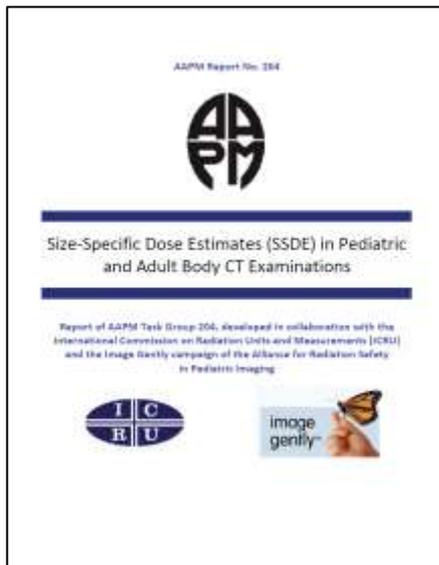
National CT DRLs (2011) for chest abdo pelvis CTDI<sub>vol</sub>= 13mGy. Therefore PET-CT DRL is 1/3 of diagnostic value.

# Results

## Dose Reduction of New Protocol

- Dose received by a patient from a CT scan is dependent on both patient size and scanner radiation output.  $CTDI_{vol}$  provides information regarding only the scanner output so does not estimate radiation dose.
- US task group 204 developed conversion factors that can be applied to displayed  $CTDI_{vol}$  to allow estimation of radiation dose for various size patients.

$$\text{Size Specific Dose Estimate (SSDE)} = CTDI_{vol} \times F$$

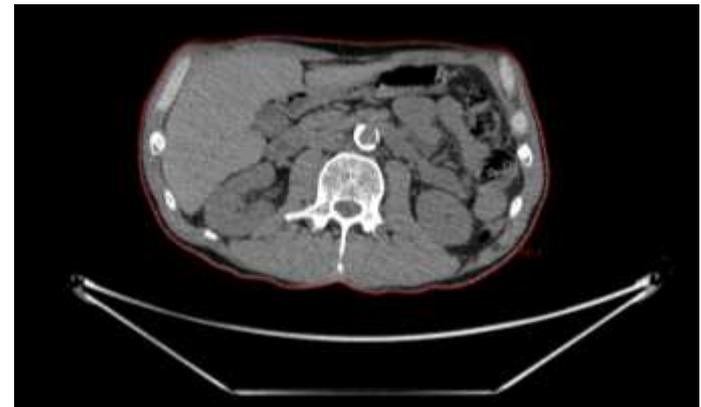
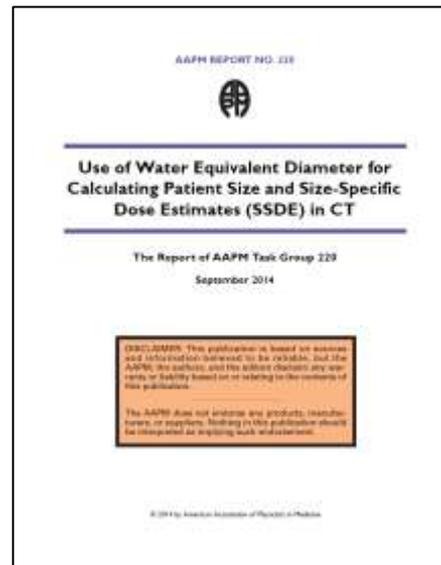
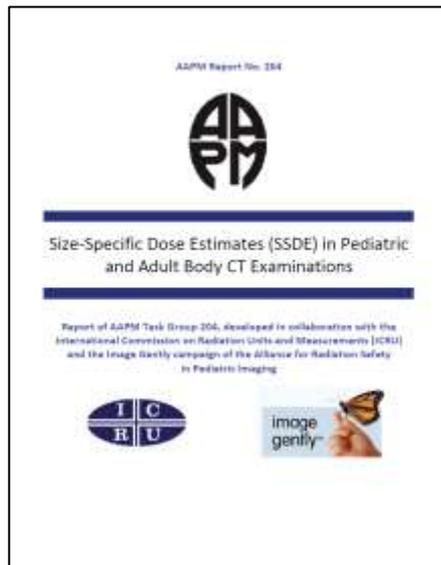


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$$\text{Size Specific Dose Estimate (SSDE)} = CTDI_{vol} \times F$$



$$D_w = 2 \sqrt{\left[ \frac{1}{1000} \overline{CT(x, y)_{ROI}} + 1 \right] \frac{A_{ROI}}{\pi}}$$

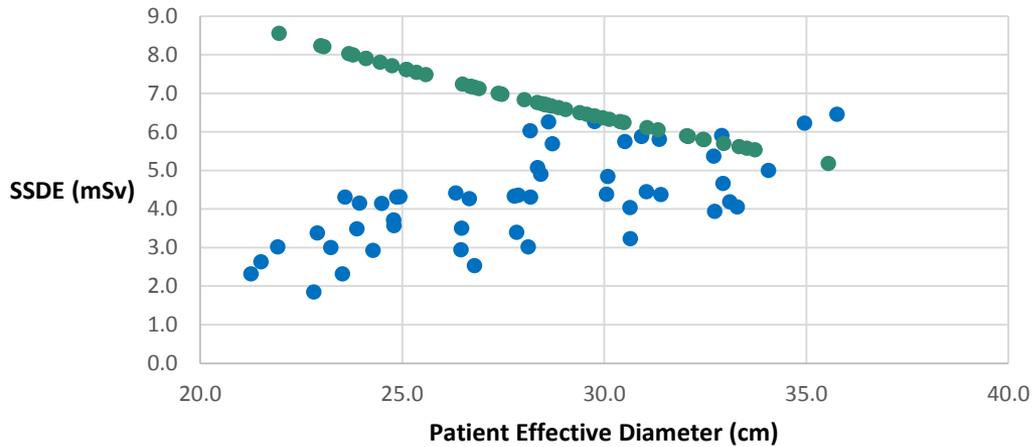
# Results

## Dose Reduction of New Protocol

TG204

Patient SSDE: Measured Effective Diameter

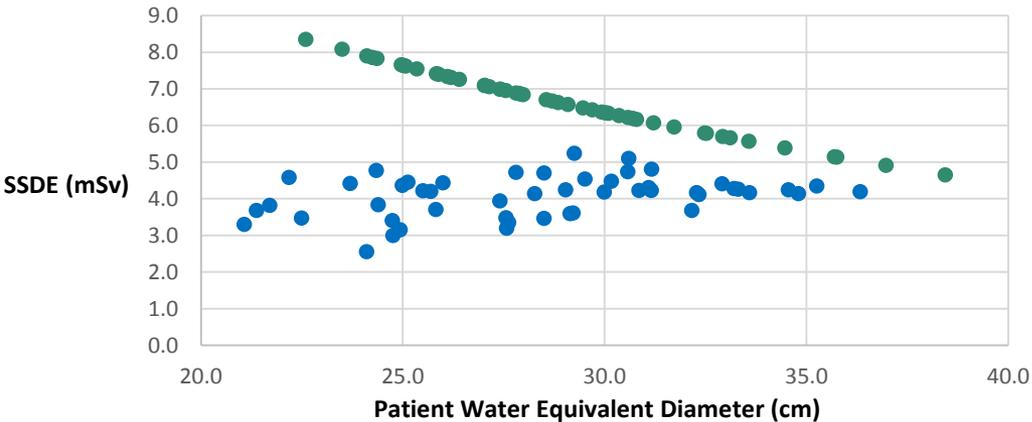
● New Protocol ● Old Protocol



TG220

Patient SSDE: Water Equivalent Diameter ( $D_w$ )

● New Protocol ● Old Protocol



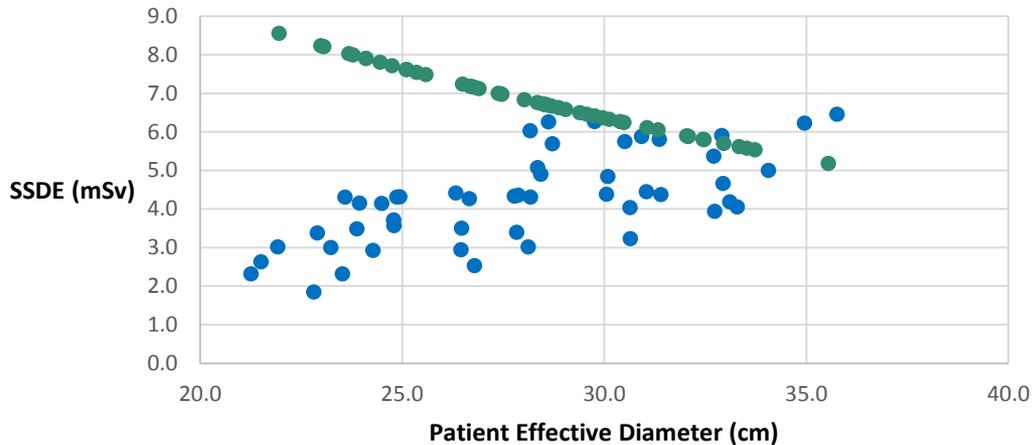
# Results

## Dose Reduction of New Protocol

TG204

Patient SSDE: Measured Effective Diameter

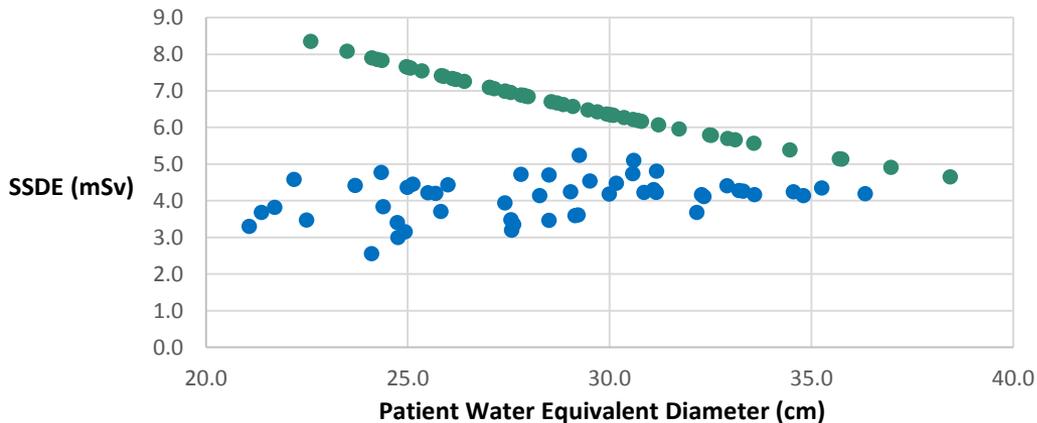
● New Protocol ● Old Protocol



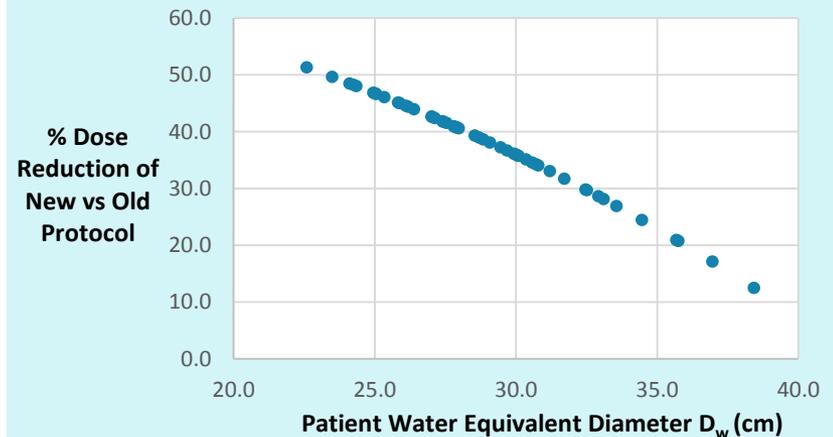
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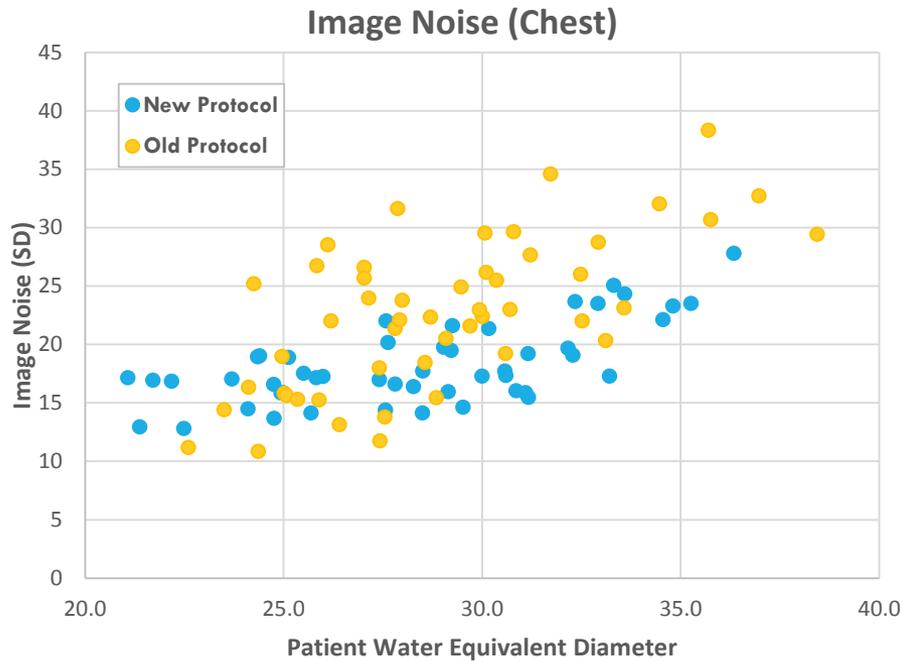
Mean % Dose Reduction with Patient  $D_w$



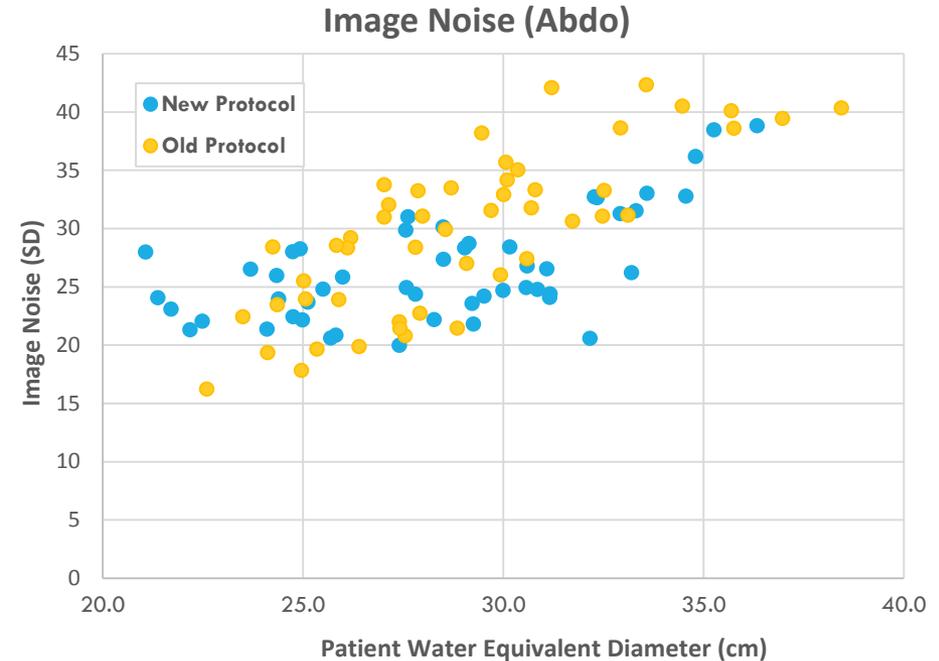
- With new protocol, doses for small patients are decreased the most

# Results

## Image Quality of New Protocol



	Mean Noise + S.D
New Protocol	19.1 +/- 3.6
Old Protocol	22.7 +/- 6.5



	Mean Noise + S.D
New Protocol	27.1 +/- 4.7
Old Protocol	29.8 +/- 6.9

- Difference in noise measurements between old and new protocols is statistically significant ( $p < 0.05$ )

# Results

## Protocol for arms up/arms down



Patient Dose	Mean DLP (1 S.D.)		Mean CTDI <sub>vol</sub> (1 S.D.)	
	Patient Arms Up	Patient Arms Down	Patient Arms Up	Patient Arms Down
<b>Old Protocol</b>	487 (65)	486 (65)	5.2 (0.0)	5.2 (0.0)
<b>New Protocol</b>	296 (79)	307 (76)	3.1 (0.8)	3.3 (0.7)

- Difference in dose metrics for arms up/arms down is not statistically significant ( $p=0.477$  (DLP) /  $0.463$  (CTDI<sub>vol</sub>))

# Results

## Phase 2: Head and Neck Local Views

# Results

## Phase 2: Head and Neck Local Views

- An additional 5 patients had reduced dose head and neck local views (mA = 70, 40% ASiR reconstruction)
- Images scored by clinicians

	Clinician 2		Clinician 3	
	Full Dose (FBP)	40% Dose + 40% ASiR	Full Dose (FBP)	40% Dose + 40% ASiR
Head and Neck 1	4	4	5	5
Head and Neck 2	4	3	3	4
Head and Neck 3	3	3	5	4
Head and Neck 4	4	3	5	4
Head and Neck 5	4	4	4	3

Scoring Scale	
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# Discussion

## How do CT doses compare with other PET-CT Sites?

	Mean DLP (mGycm)	Mean Image Noise (HU)	Slice Thickness (mm)
<b>St Thomas' PET Centre</b>	302	27.1	2.5
<b>Manchester/Leeds PET-CT 1 (GE)</b>	306	22.4	3.75
<b>Manchester/Leeds PET-CT 2 (Siemens)</b>	197	42.1	4
<b>Manchester/Leeds PET-CT 3 (Philips)</b>	385	15.2	4
<b>Manchester/Leeds PET-CT 4 (Philips)</b>	296	19.7	4

G Iball and D Tout, *Computed Tomography Automated Exposure Control Techniques in 18F-FDG Oncology PET-CT Scanning*, Nuc Med Comm 2014, Vol 35 No 4

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## CT for PET Attenuation Correction?

mAs	Activity Concentration (Bq/ml)
10	5767
15	5769
20	5769
25	5759
30	5762
35	5763
40	5763

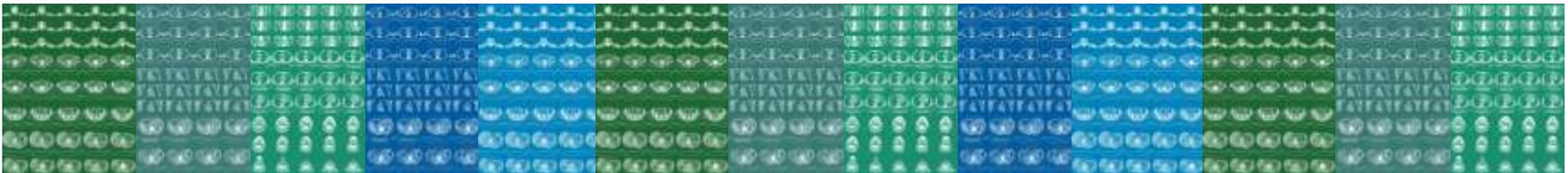
# Conclusions

- Mean effective half-body CT dose in PET-CT reduced to 4.2mSv. Therefore CT component is now ~38% of total PET-CT dose.
- Image Quality has received no complaints. Image noise measured in torso is lower than previous protocol.
- Possibility of reduction of mean effective head and neck CT dose from 1mSv to 0.6mSv.



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- Image Quality has received no complaints. Image noise measured in torso is lower than previous protocol.
- Possibility of reduction of mean effective head and neck CT dose from 1mSv to 0.6mSv.
- Other sites already have lower doses than us without ASiR. What image quality is deemed sufficient for localisation scans? Potential to go lower?
- All PET-CT scanner manufacturers have iterative reconstruction capabilities. Therefore further dose reduction in CT in PET envisaged in future.
- National dose audit would be extremely useful so as to know where we rank and what to aim for.



# Full dose vs Reduced dose images?

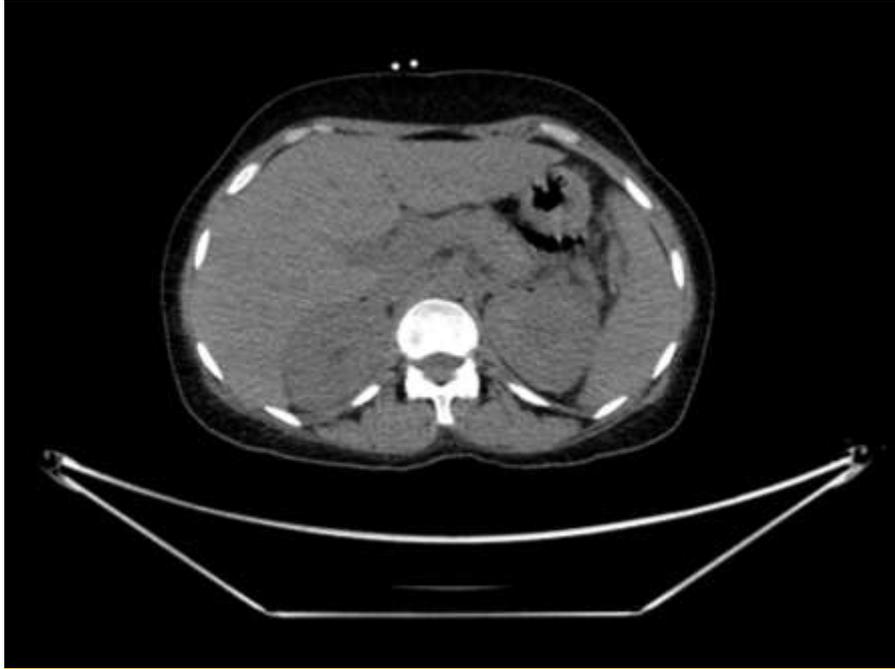


**21% Dose Reduction**

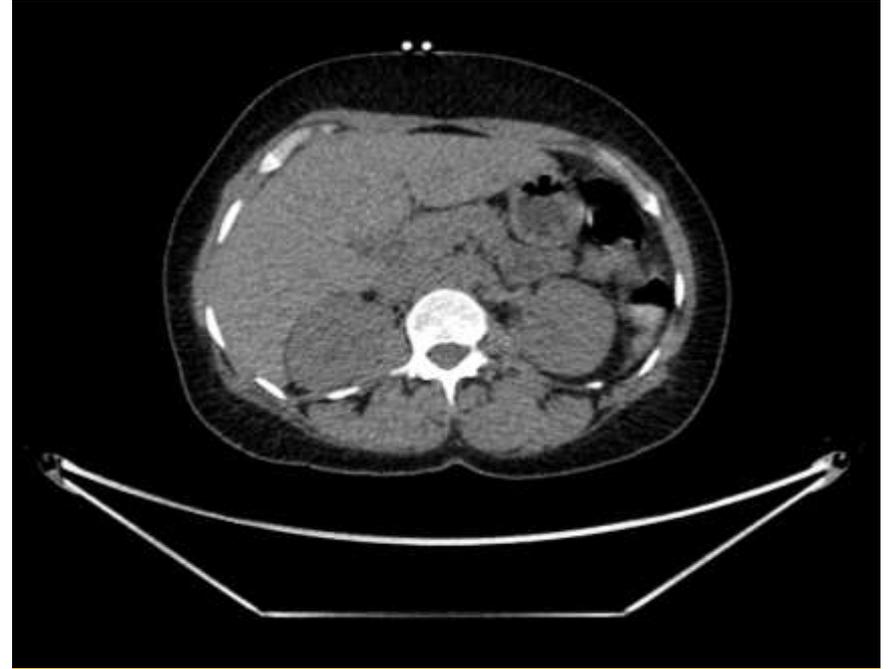


**Old Protocol**

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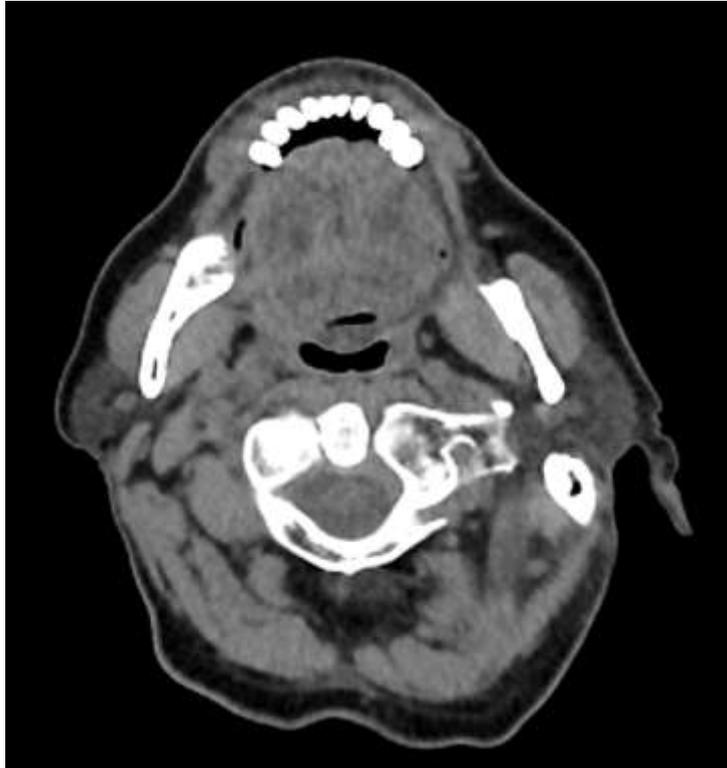


**Old Protocol**

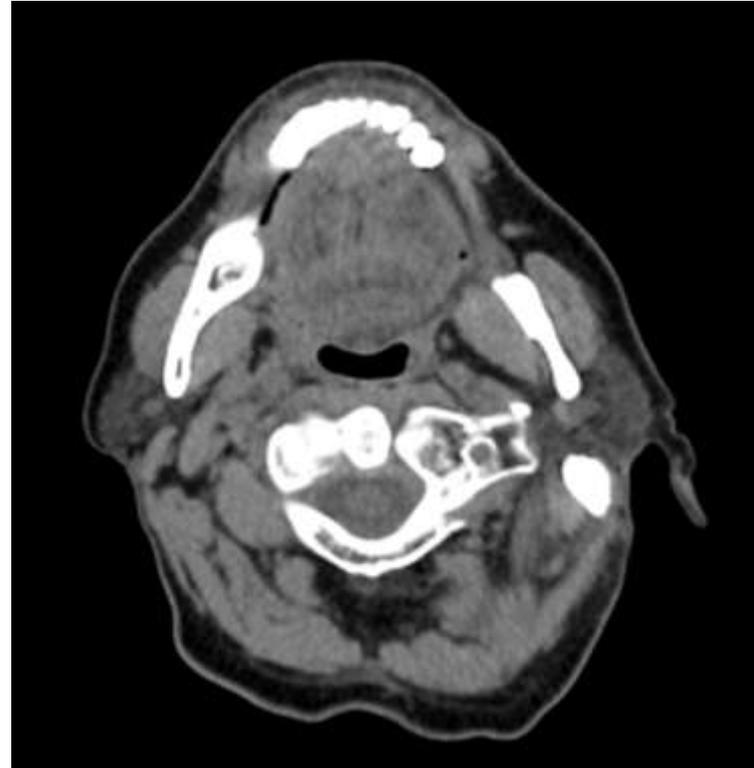


**48% Dose Reduction**

# Full dose vs Reduced dose images?



**40% Dose Reduction**



**Old Protocol**